SENSORS in the field of SLEEP

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PSG in History

- · 1875: Discovery of brain-wave activity
- 1930: Description of differences between the waking and sleeping states
- 1937: A correlation between apparent behavioural sleep and EEG documentation of sleep.
- 1947: Recommendation to further study sites of recording brain activity.
- 1953: Inclusion of electro-oculography (EOG)
- 1957: Discovery of rapid eye movements during sleep with episodes of completely activated EEG

PSG in History continued

- 1957: Eye movements related to dream activity
- 1958: International 10-20 (%) system of electrode placement was developed (23 electrode sites)
- 1959: EMG muscle tone suppressed in REM
- 1968: Standardized terminology, techniques and scoring for sleep stages (R &K) developed
- · 1974: Term polysomnography (PSG) was proposed
- 1978: Routine PSG consisted of EEG, EOG, EMG (mentalis, submentalis), EMG (tibialis) ECG, oxygen saturation, nasal airflow and rib cage and abdominal respiratory effort









The PSG (Polysomnogram)

- The primary function of the PSG is to allow us to record and monitor bioelectric activity of the body.
- The signals from the cortex and from other sites are extremely small voltages (some micro volts).

The PSG continued

- In addition the PSG allows us to accentuate or optimize a signal by filtering out data that are not relevant to the signal of interest. The frequency ranges required is determined by assessing the recorded frequencies and determining the frequencies of extraneous potentials we wish to eliminate.
- We need to amplify and record the differences in potentials between two inputs and simultaneously compare them to a reference.

The PSG continued

- For example in a limb channel we wish to record high frequency muscle potentials but have no interest (for that channel) in low frequency potentials like slow respiratory movements.
- We set the filters such that the high frequency potentials "pass through" and the lower frequency extraneous potentials are "filtered out".
- We then accentuate the selected signal (limb muscle bursts) by selecting an appropriate sensitivity to display the signal in a meaningful, readable amplitude.

Edit Imp	od Filters	() Patient	O Video	New New Record	6			- out	
· C Data Type	8		Name	Input Type	Rate	Coupling	HP Filter	P.P.Range	Imp. C
- EE Physical C	hannels	1	Off	AC Bectrode (Ch 1-32	0	AC	0.15	1 mV	740
Trace Par	es	2	Bipolar	AC BPolar (Ch 33-40)	64	AC	0.05	1 mV	No
- Pane	1 Traces	3	Oximeter	Oximeter (Ch 45-47)	1	DC .	0	Direct	No
Pane Pane	2 Traces	4	EE0	AC Electrode (Ch 1-32	128	AÇ	0.15	1 mV	Yes
E- Filters		5	ECO.	AC Bectrode (Ch 1-32	128	AC	0.15	4 nV	Yes
🚽 🖉 Data	ypes	6	DM0	AC Electrode (Ch 1-32	256	AC	0.15	1 mV	Yes
Trace		7	Pressure	Pressure	64	DC	0	2 V	No
E-G2 Sleep Ana	6yexe	8	Flow	Airflow	256	AC	0.05	2 ¥	No
		9	DC	DC BPolar (Ch 41-44)	1	DC	0	512 mV	No
		10	External DC	DC Non-Isolated	4	DC	0	2 V	No
		11	Sound	AC BPolar (Ch 33-40)	128	AÇ	0.05	1 mV	No
		12	Leg	AC BPolar (Ch 33-40)	128	AC	0.05	64 mV	No
		13	Effort1	AC BPolar (Ch 33-40)	64	AC	0.05	0 nV	No
		14	Effort2	AC BPolar (Ch 33-40)	64	AÇ	0.05	8 mV	No
		15	bipolar2	AC BPolar (Ch 33-40)	256	AC	0.05	1 mV	No
		16							







































Sleep Sensors continued.

tcO2

For the pO2 reading oxygen diffuses to the platinum cathode through the electrodes membrane. A reduction in oxygen occurs as a result of the current generating process. This reduction generates a current which is fed into the pO2 channel and converted to a voltage, digitalized then passed to the micro computer and displayed.

tcCO2

The pCO2 measurement is a pH measurement. As CO2 is released from the skin it diffuses into the electrolyte. It reacts with water forming carbonic acid and immediately dissociates by the following equation.

The changes in H in the electrolyte imply changes in pH. As the pH in the electrolyte changes, the voltage between the glass electrode and reference electrode changes. This change is converted to pCO2 by the Henderson Hasselbach equation. The signal is then digitalized.

Process

- With all signals you do not just plug the sensor in and display the recording.
- The signal is amplified (Pre Amps/ Amps)
- Then filtered for different types of noises. (Filters)
- Then the signal is displayed on a monitor.
- There are different amplifiers and filters depending on the voltage, frequency and amplitude of the physical signal.









Problems we encounter

- · ECG interference
- Respiratory
- Perspiration
- Body motion
- · Defective electrodes
- Electrical interference
- · Restriction due to wiring
- · How accurate as not a "normal nights sleep"











Present Developments

- Oximetry
 - Blue tooth technology
- Eye blinking
 - Car engine turns off if sleepy or car horn sounds
- Algorithms

 Daily improvement
- Telemedicine
 - Continually scan the patient

Future

- Improvement of treatment options

 auto adjusting CPAP relatively new
- Better algorithms for measuring all signals
 - reduce manpower and improve accuracy
- External lab systems – Telemedicine main option



How could you help us?

- To fine tune our present technology
- The development of new sensors / techniques / equipment
- Help with specialized research requirements
- The future of the development on the measurement of physical sensors is with you
- What is your dream or idea???? – We are all ears and we are waiting!!!!

Like to Visit ?

- If you would like to observe a sleep study at night or visit us during the day you are most welcome.
- · Please call us on 8345 6124 to arrange

